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ADAPTIVE ACQUISITIONS IN BIOMEDICAL OPTICAL IMAGING BASED ON SINGLE PIXEL CAMERA: COMPARISON WITH COMPRESSIVE SENSING

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I. Introduction

II. State of the art

II.1 – Compressive sensing

II.2 – Adaptive acquisition

III. Proposed acquisition strategy: ABS-WP

III.1 – Wavelet decomposition

III.2 – ABS-WP strategy

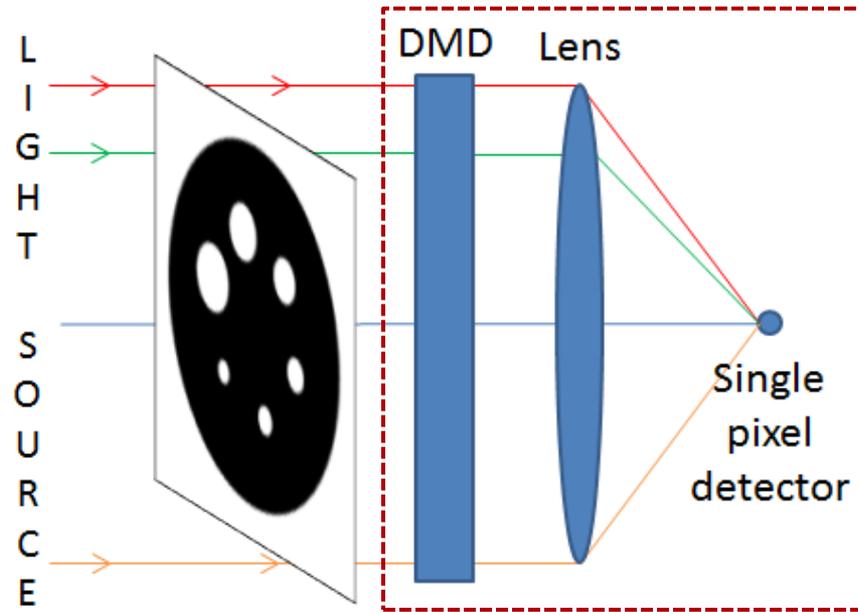
IV. Results and comparisons

IV.1 – Simulations on real images

IV.2 – Experimental data

V. Conclusion

I. Introduction

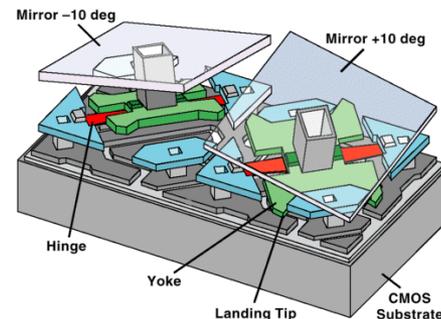


Single-pixel camera (SPC)

- **DMD:** millions of mirrors that can independently tilt in two positions → can be used as a **spatial filtering device**



Digital micro-mirror device

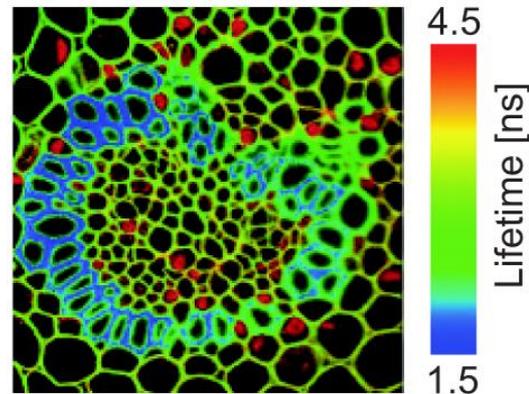


Two mirrors of 13.7 μm (Texas Instruments)

➤ Several advantages:

- **Infrared** or **multispectral** imaging
- **High quantum efficiency**: able to detect weak intensity light changes
- **Low cost** time-resolved system (one photon counting board)

Fluorescence lifetime imaging (PicoQuant)



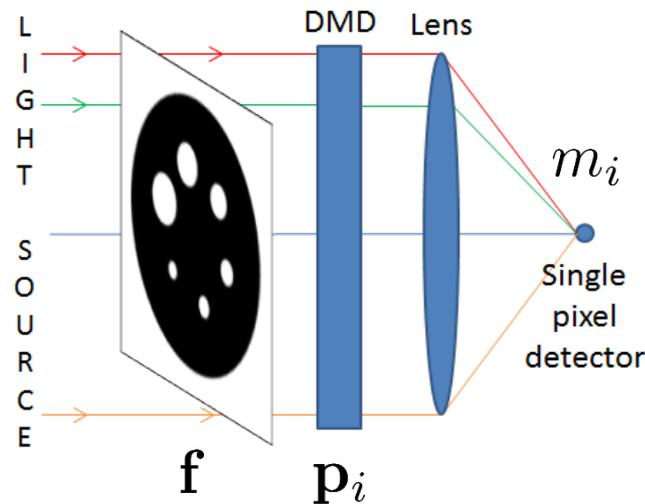
➤ Possible **applications in medical imaging**:

- Fluorescence molecular tomography [*Intes 2015*]
- Fluorescence lifetime imaging
- Per-operative imaging (oxygenation or fluorescence)

➤ SPC acquisition:

- Image of size $N \times N = P$ $\mathbf{f} \in \mathbb{R}^{P \times 1}$
- I patterns of size $N \times N = P$ $\mathbf{p}_i \in \mathbb{R}^{P \times 1}$

→ I measures m_i with $m_i = \mathbf{f}^\top \mathbf{p}_i$



➤ Problems:

- P1 – Choice / design of the patterns \mathbf{p}_i
- P2 – Restoration of the image \mathbf{f} from the measures m_i knowing \mathbf{p}_i

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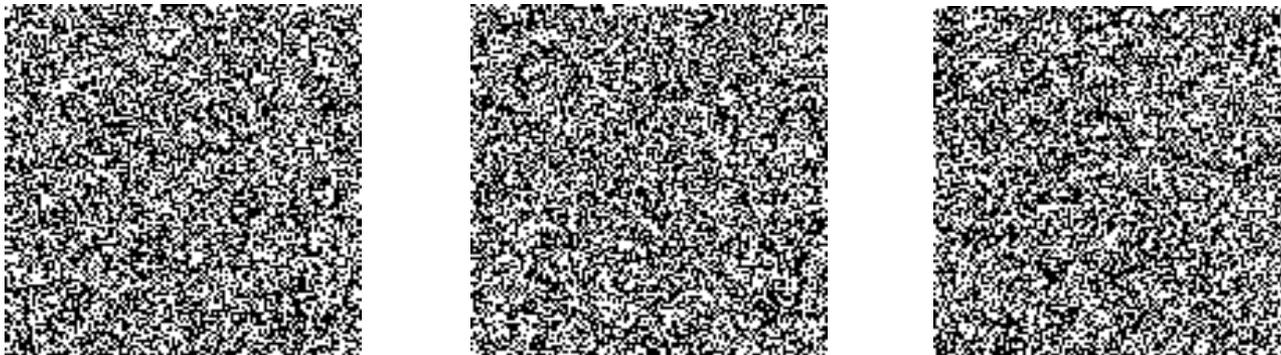
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II.1 – Compressive sensing

- Acquisition based on the **compressive sensing (CS)** [Donoho 2006, Duarte 2008]
- P1 – Patterns chosen as independent realizations of **random ± 1 Bernoulli variables**
- P2 – Perfect restoration, in theory, by l_1 -minimization in a basis (e.g. wavelets). In practice: **TV-minimization** (Total Variation) for faster image recovery [Takhar 2006, Duarte 2008]

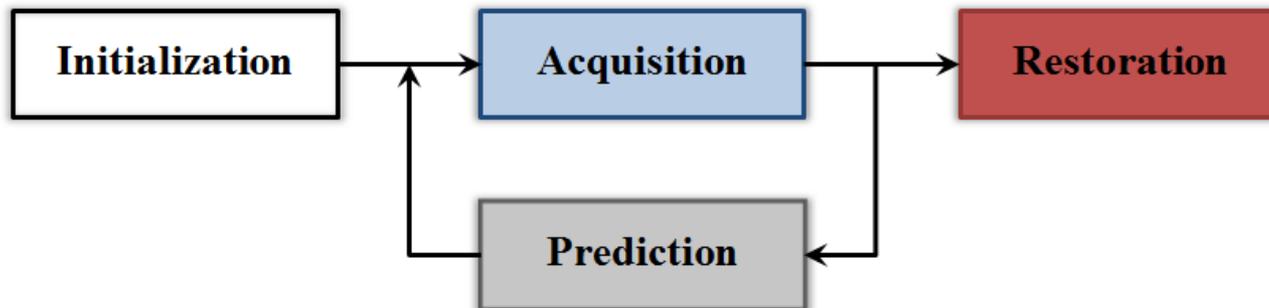


Example of 3 random patterns

- **Non-adaptive** approach: same set of patterns regardless of the image

II.2 – Adaptive acquisition

- **Acquisition directly in a given basis** (Fourier, DCT, wavelets, etc...) [*Deutsch 2009, Averbuch 2012, Dai 2014*]
- P1 – Patterns of the chosen basis, some are **determined during the acquisition** based on measures already performed (prediction step)
- P2 – Almost **instant image restoration** using the chosen basis inverse transform [*Mallat 2008*]



General framework of an adaptive approach

- **Adaptive** approach: different set of patterns depending on the object

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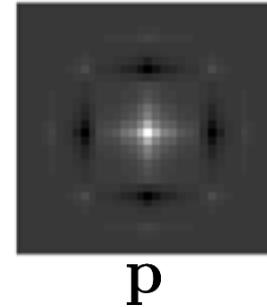
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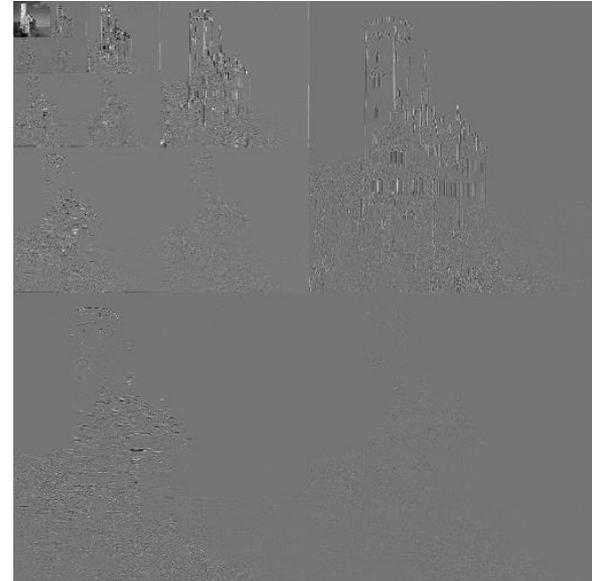
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III.1 – Wavelet decomposition

- Choice of an **adaptive** approach in the wavelet domain
- Coefficient: $c = \mathbf{f}^\top \mathbf{p}$ \Leftrightarrow one SPC measurement
- Non-linear approximation: retains a given percentage of the **strongest coefficients** and shows excellent image recovery [Mallat 2008]



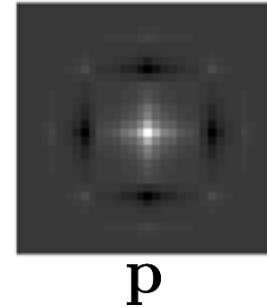
Ground truth 512 x 512 image



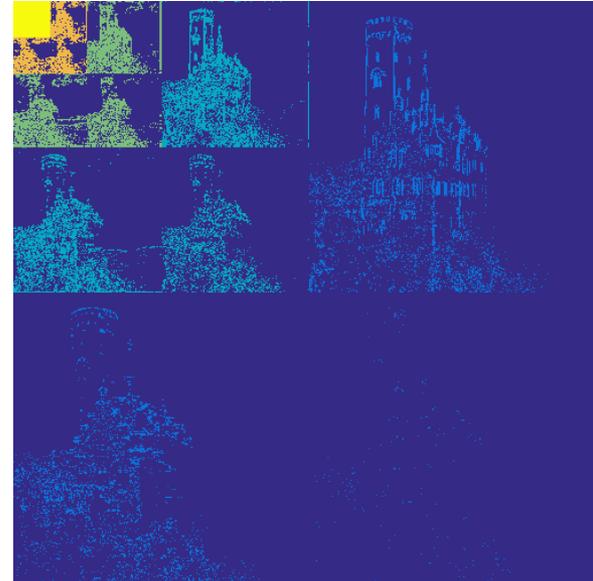
4-level wavelet decomposition

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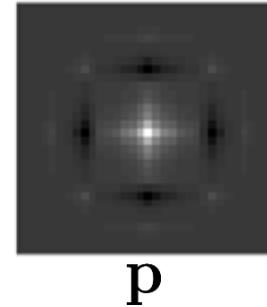
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10% of the strongest coefficients

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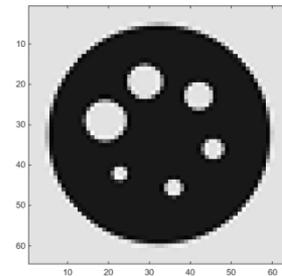
Restored image with 10% of the coefficients

III.2 – ABS-WP strategy

- **ABS-WP**: Adaptive Basis Scan by Wavelet Prediction [*Rousset 2015 - 2016*]
- **Multiresolution** approach: non-linear approximation idea applied on each of the $j = 1 \dots J$ scales of the J -level wavelet decomposition

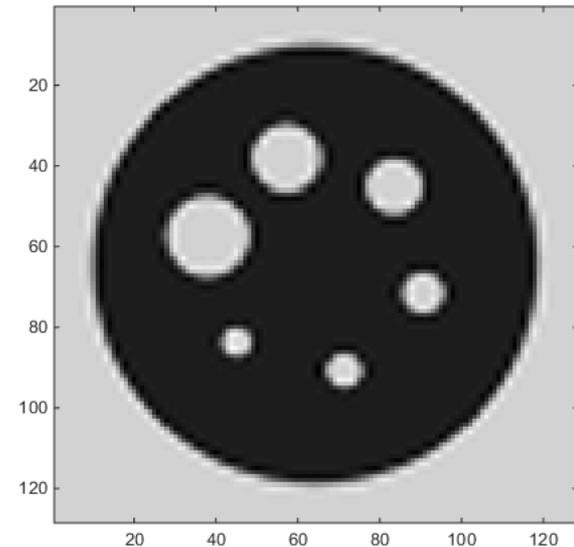
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 - 1 – Approximation image acquisition



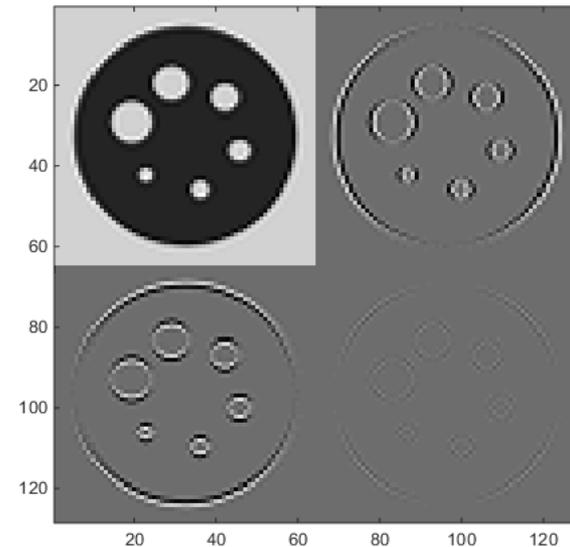
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 - 2 – Over-sampling by a factor 2 by a bi-cubic interpolation [*Keys 1981*]



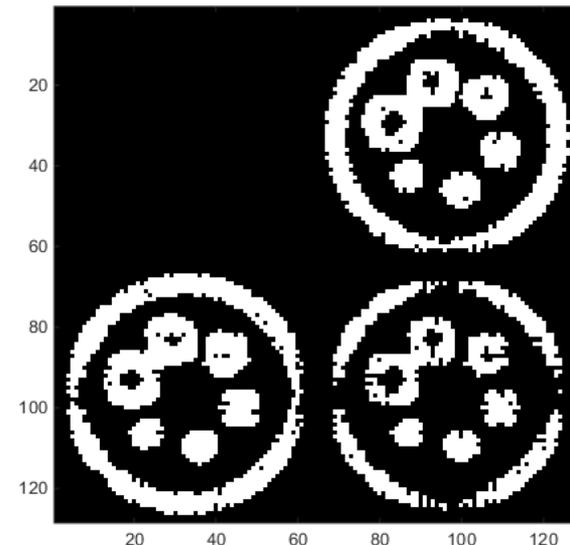
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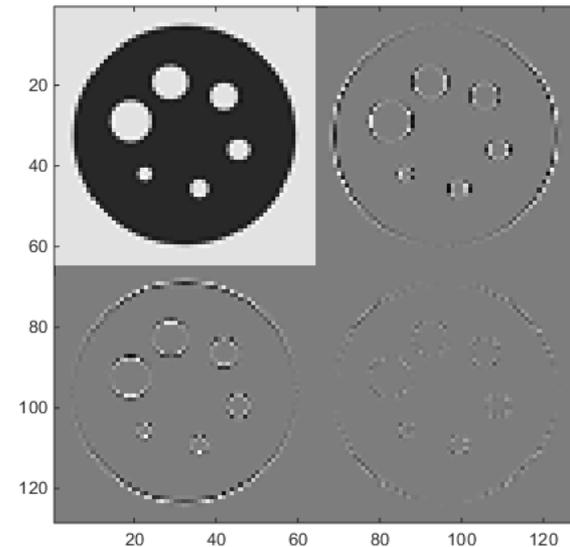
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 - 4 – A percentage p_j of the strongest detail wavelet coefficients is retained



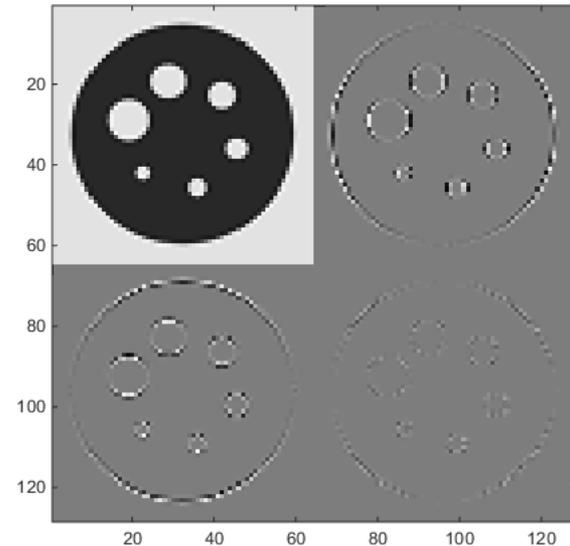
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 - 5 – The “predicted” significant coefficients are experimentally acquired



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- Set of percentages $\mathcal{P} = \{p_J, \dots, p_1\}$ to control the compression rate (CR)

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IV. Results and comparisons

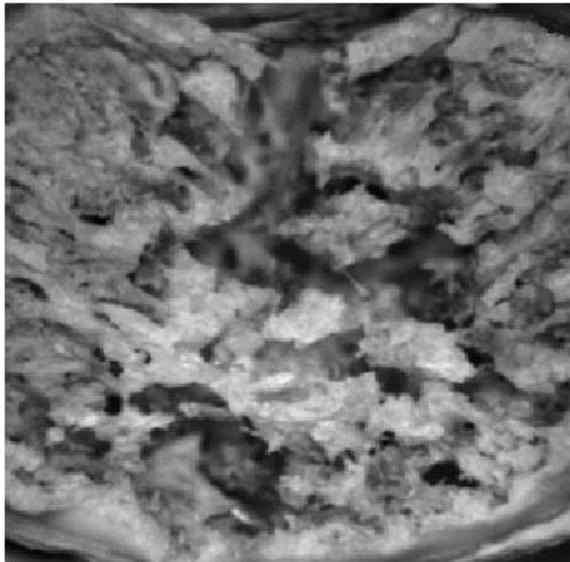
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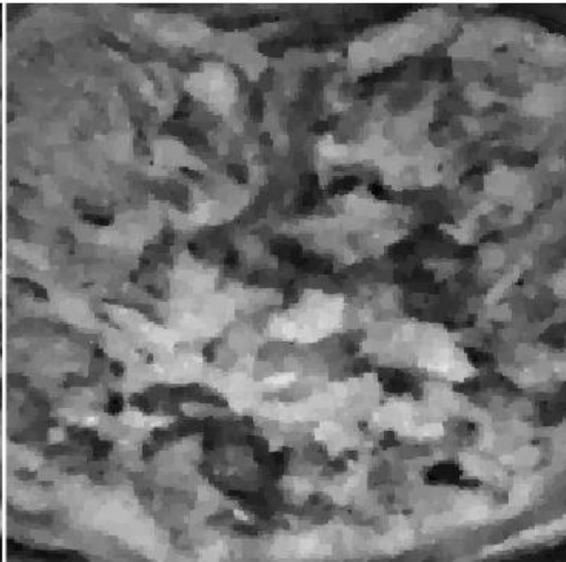
V. Conclusion

IV.1 – Simulations on real images

- Histological image of bone structures
- Simulations for **CR = 80 %**
 - CS : restoration by TV-minimization
 - ABS-WP : Le Gall's wavelet employed (CDF 5/3)



Reference 256 x 256



CS

PSNR = 29.4 dB

t = 214 s



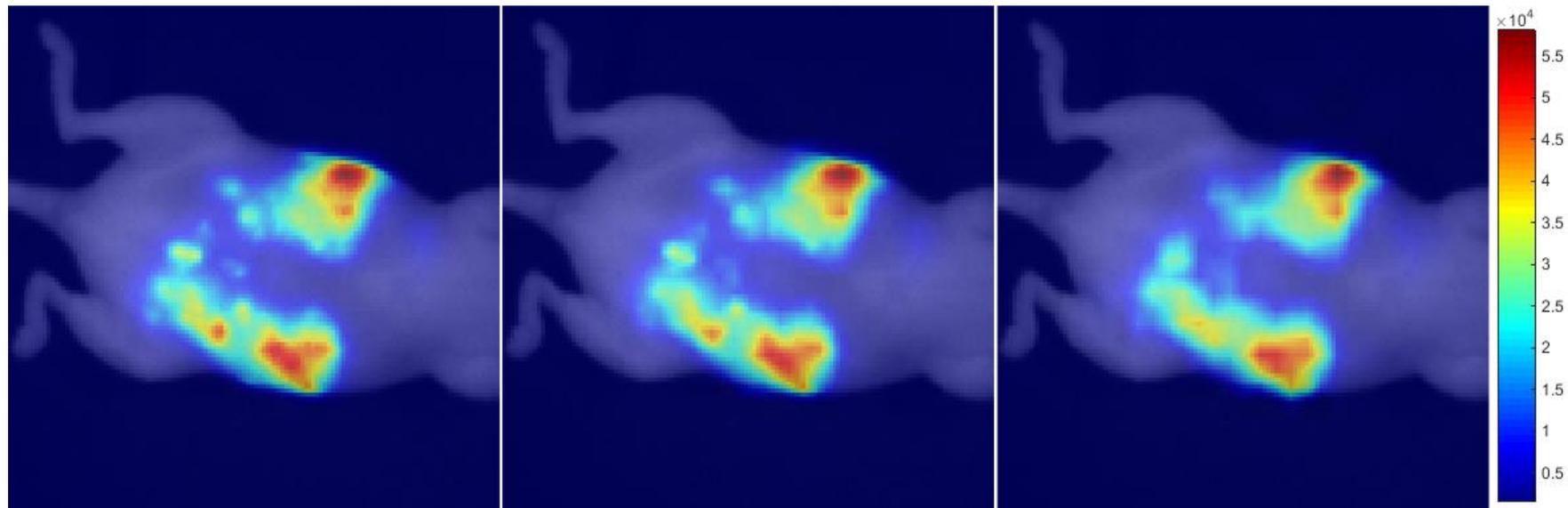
ABS-WP

PSNR = 31.2 dB

t = 0.4 s

IV.1 – Simulations on real images

- Bioluminescence image of a mouse over the ambient light image (images provided by V. Josserand et J.L. Coll) [Coll 2010]
- **ABS-WP** simulations (Le Gall) on the bioluminescence image:



Reference 128 x 128

CR = 95 %
PSNR = 41.2 dB

CR = 98 %
PSNR = 35.3 dB

- **High compression rates for smooth images**

IV.1 – Simulations on real images

- **PSNRs** obtained for 4 tests images for **CS** or our method **ABS-WP** for a **85 %** compression rate:

Image	PSNR (dB)	
	CS	ABS-WP
Lena (256 x 256)	27.89	29.59
Peppers (256 x 256)	32.96	34.83
Bone structures (256 x 256)	28.14	30.29
Mouse (128 x 128)	41.41	48.58

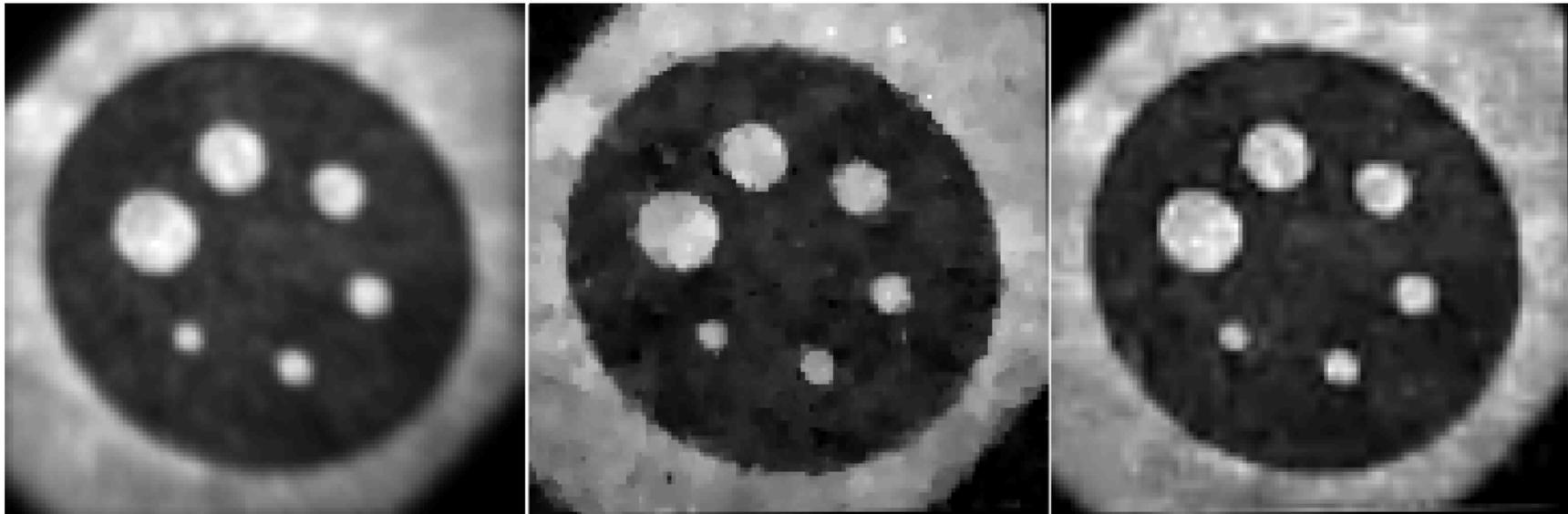
- **Set of percentages** used for ABS-WP **identical** for each image:

$$\mathcal{P}_{85\%} = \{0.90, 0.80, 0.45, 0.019\}$$

- **Adaptivity** of ABS-WP to different types of images

IV.2 – Experimental data

- Jaszczak target printed on a paper and then employed as object
- Acquisitions for **CR = 80 %**
 - CS : restoration by TV-minimization
 - ABS-WP : Le Gall's wavelet



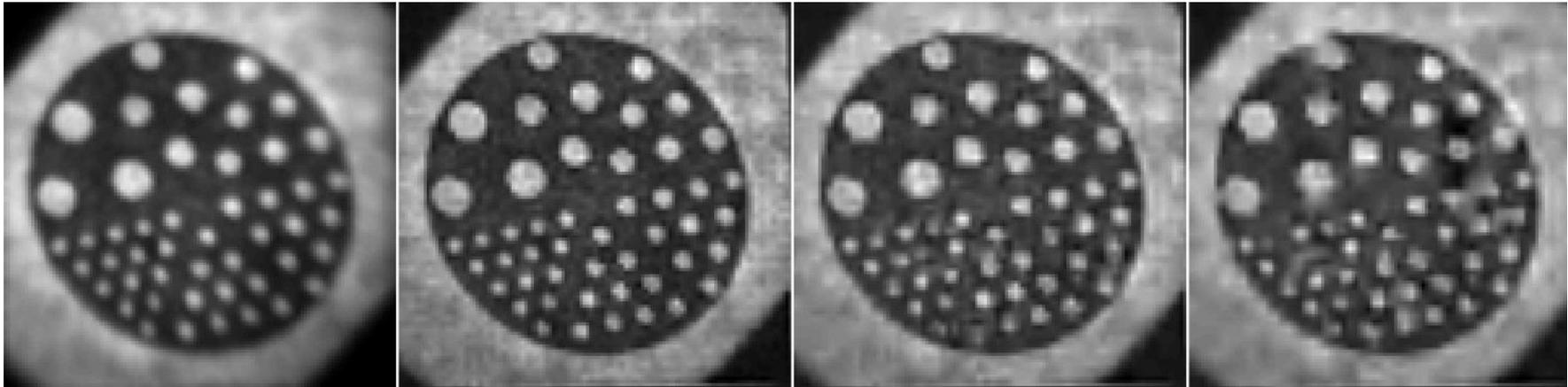
Experimental CCD
128 x 128 image

CS
PSNR = 21.2 dB
t = 14 s

ABS-WP
PSNR = 21.7 dB
t = 0.2

IV.2 – Experimental data

- Other Jaszczak target printed on paper and employed as an object to judge the system's spatial resolution. $\varnothing = [1; 3]$ mm
- Acquisitions for **ABS-WP** (Le Gall) :



Experimental CCD
128 x 128 image

CR = 75 %
PSNR = 22.4 dB

CR = 85 %
PSNR = 21.5 dB

CR = 90 %
PSNR = 20.9 dB

- Measured pixel pitch of **210 μm** . It can be easily modified by changing the optics or the size of the patterns.

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➤ Proposed method to acquire images by a SPC:

- **Adaptive** technique
- **Wavelet** patterns
- Bi-cubic interpolation **prediction**
- **Multiresolution** approach

➤ **Favorable** comparison with compressive sensing:

Type of comparison	CS	ABS-WP
Restoration	Perfect in theory	Perfect if CR = 0%
Complexity	Expensive computation	Direct restoration
Computation time	x 10-100	1
Parameters	Several parameters for the TV-minimization	Choice of the wavelet + set of percentages

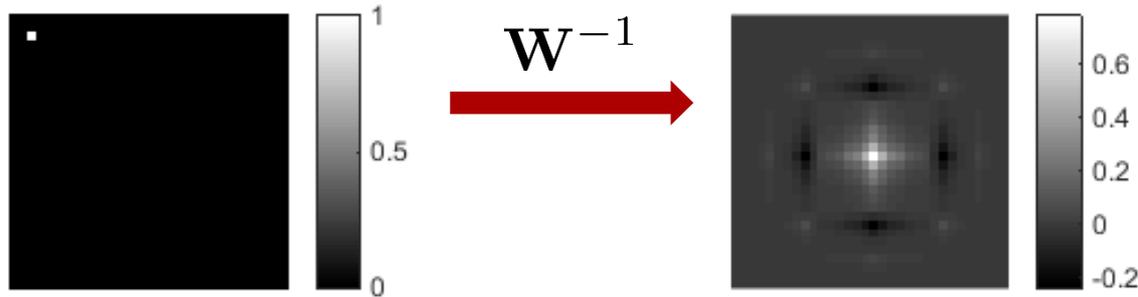
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- We note \mathbf{W} an orthonormal operator so that one wavelet pattern \mathbf{p} can be obtained as

$$\mathbf{p} = \mathbf{W}^{-1} \mathbf{e} \quad \mathbf{W} \in \mathbb{R}^{P \times P}$$

with \mathbf{e} a unit vector chosen from the canonic basis :



- Obtained patterns have real positive and negative values. The DMD can only receive b-bits patterns

→ **uniform quantization** of the patterns and positive/negative separation:

$$q_f = \frac{\max(|\mathbf{p}|)}{2^b - 1} \quad \hat{\mathbf{p}} = \left\lfloor \frac{1}{q_f} \mathbf{p} \right\rfloor \quad c \approx q_f \mathbf{f}^\top \hat{\mathbf{p}} = q_f (\mathbf{f}^\top \hat{\mathbf{p}}^+ - \mathbf{f}^\top \hat{\mathbf{p}}^-)$$

- **Average computation times** for the simulations + experimental data (acquisition time excluded). It includes TV-minimization for CS and the prediction step + restoration for ABS-WP :

Image size	Time (s)	
	CS	ABS-WP
128 x 128	13.18	0.18
256 x 256	213.62	0.42

- **TV-minimization** demands **expensive computations**, time increases quickly with the number of measures and the image size
- For ABS-WP, **bi-cubic interpolation** and the **wavelet transform** are **optimized** and **fast** operations
- **Real time** possible for our technique