



(A short intro to) Deep learning for image reconstruction

Nicolas Ducros^{1, 2}

¹CREATIS, Univ Lyon, INSA-Lyon, UCB Lyon 1, CNRS, Inserm, CREATIS UMR 5220,
U1206, Lyon, France

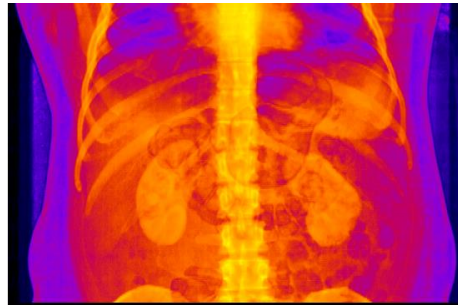
²IUF, Institut Universitaire de France

“Natural” vs Reconstructed images

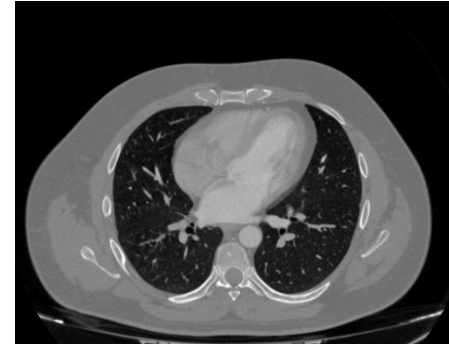
Rec



Nat



Rec



Nat



Nat



Rec



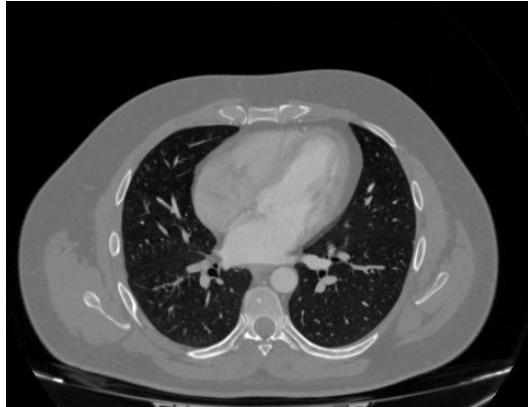
Nat



Nat



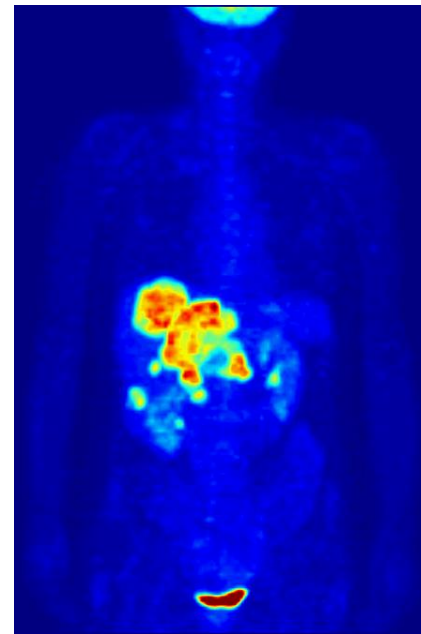
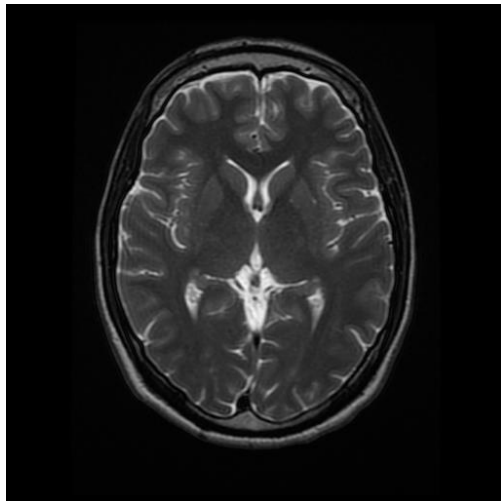
Computerized tomography (CT)



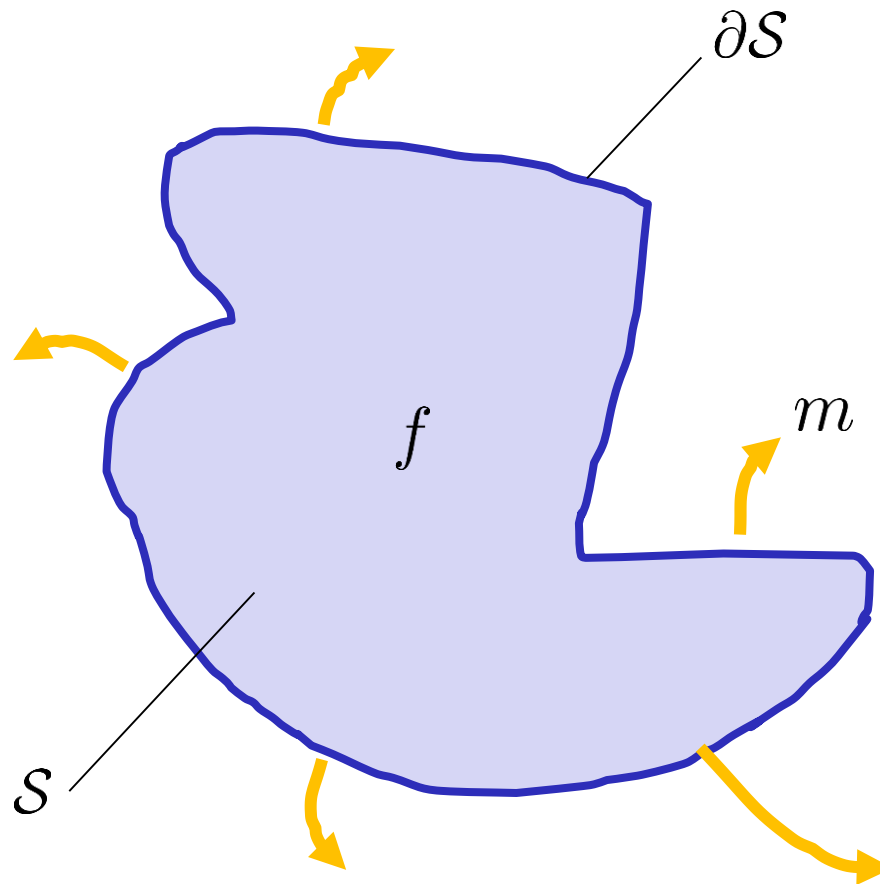
Ultrasound Imaging



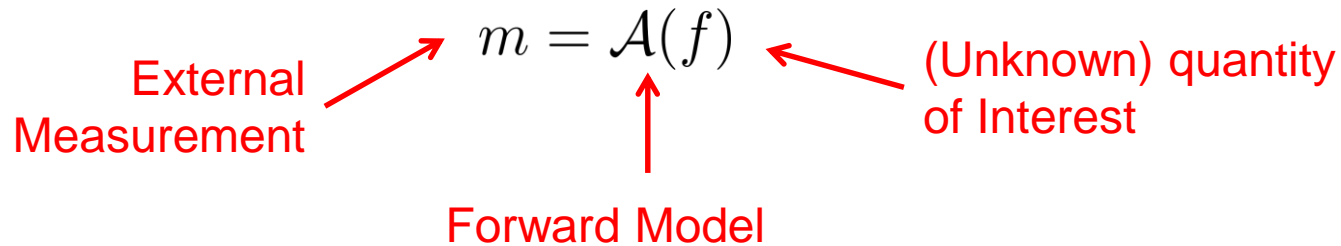
Magnetic Resonance (MRI)



Positron emission tomography (PET)



➤ **Internal unknowns from external measurements**



➤ **Most medical imaging problems are**

- ❖ Linear
- ❖ Corrupted by noise

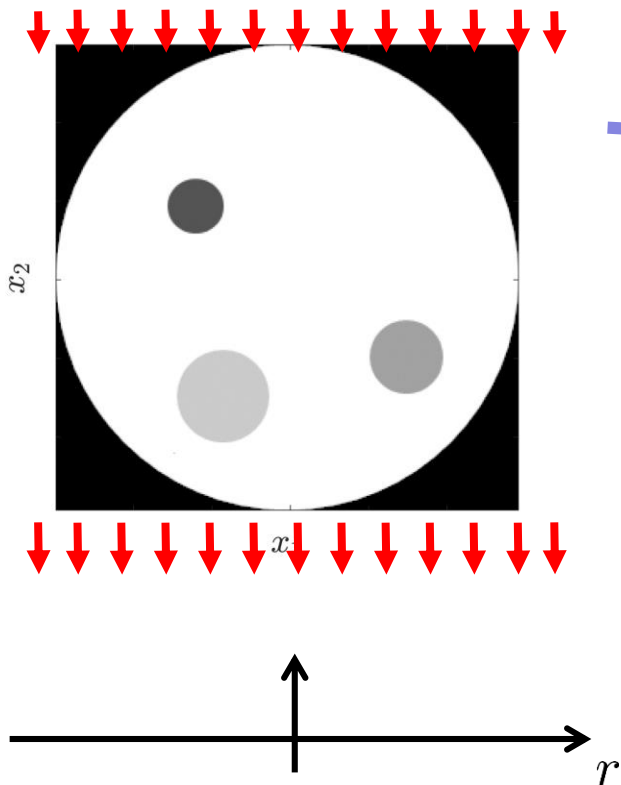
➤ **In a discrete setting**

$$m = \mathbf{A}f + \eta$$

$m \in \mathbb{R}^M$ \leftarrow $\mathbf{A} \in \mathbb{R}^{M \times N}$ $f \in \mathbb{R}^N$ \leftarrow Noise

The diagram shows the discrete forward model equation $m = \mathbf{A}f + \eta$. Red arrows point from the labels $m \in \mathbb{R}^M$, $\mathbf{A} \in \mathbb{R}^{M \times N}$, and $f \in \mathbb{R}^N$ to their respective terms in the equation. A red arrow labeled "Noise" points from the right towards the term η .

CT slice (unknown)

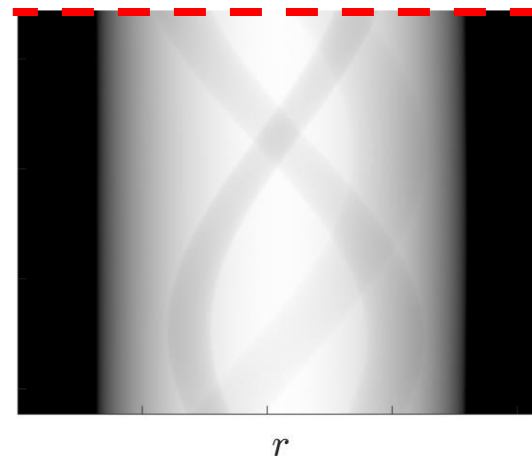


$$m(\theta, r) = \mathcal{R}[f](\theta, r)$$

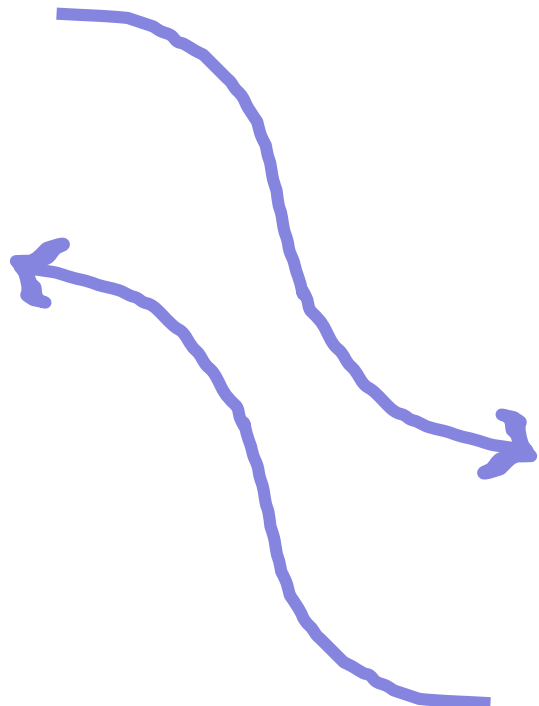
$$= \int_{\mathcal{L}(\theta, r)} f(x_1, x_2) dl$$

$\theta = 0$

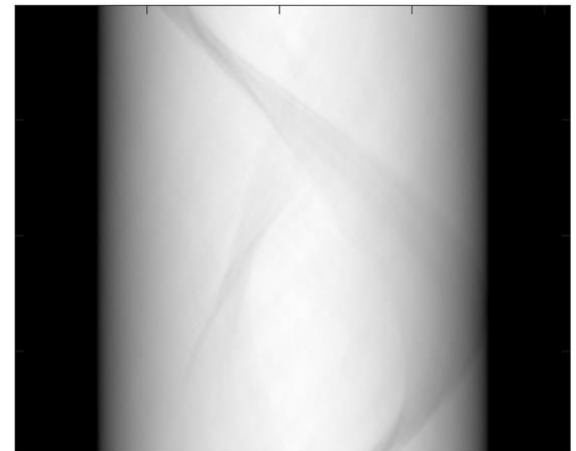
Sinogram (measured)



CT slice (unknown)



Sinogram (measured)



➤ **1. Inversion “by hand”**

- ❖ Model the forward and try to invert algebraically

derive \mathcal{H} such that $f = \mathcal{H}(m)$

➤ **2. Optimization of handcrafted functionals**

- ❖ Build cost function from prior knowledge about the solution/measurements
- ❖ Minimize the cost function

find and minimize \mathcal{C} such that $\mathcal{C}(f; m)$ is small

➤ **3. “Learn” to reconstruct**

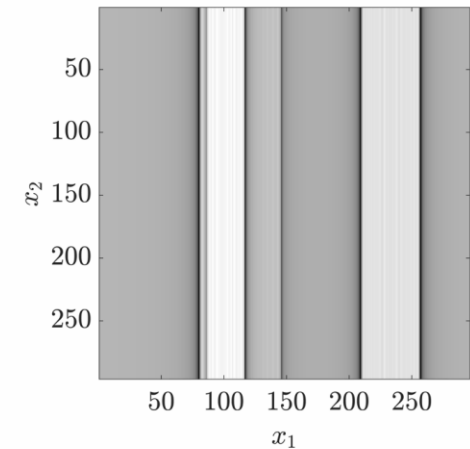
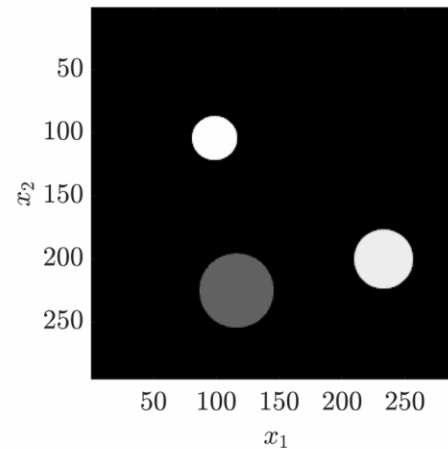
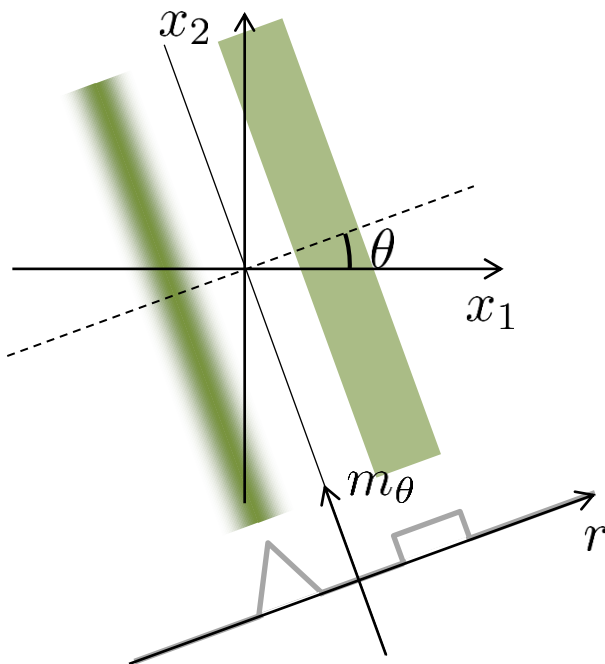
- ❖ (Probably what you expect from this talk)

learn \mathcal{H}_ω such that $f = \mathcal{H}_\omega(m)$

➤ Example with CT (filtered backprojection)

$$f(x_1, x_2) = \int_0^\pi m_\theta^{\text{filt}}(x_1 \cos \theta + x_2 \sin \theta) d\theta$$

$$\hat{m}_\theta^{\text{filt}}(\xi) = |\xi| \hat{m}_\theta(\xi)$$



➤ Pros

- ❖ Elegant
- ❖ Theoretical guarantees
- ❖ Usually fast implementation

➤ Cons

- ❖ Not always possible to derive a solution
- ❖ Influence of noise?
- ❖ What if only few measurements are available?
 - For dose reduction/short scans
 - Short scans are less prone to motion artefacts

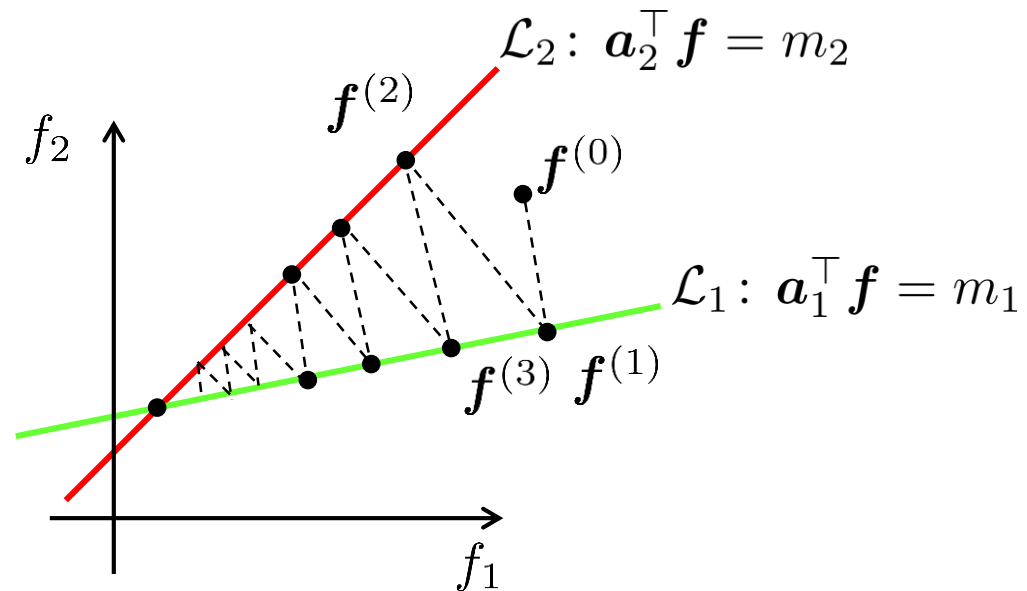
- Look for an image with small residuals

$$r = m - Af \approx 0$$

❖ A simple example:

$$\begin{bmatrix} m_1 \\ m_2 \end{bmatrix} = \begin{bmatrix} a_{1,1} & a_{1,2} \\ a_{2,1} & a_{2,2} \end{bmatrix} \begin{bmatrix} f_1 \\ f_2 \end{bmatrix}$$

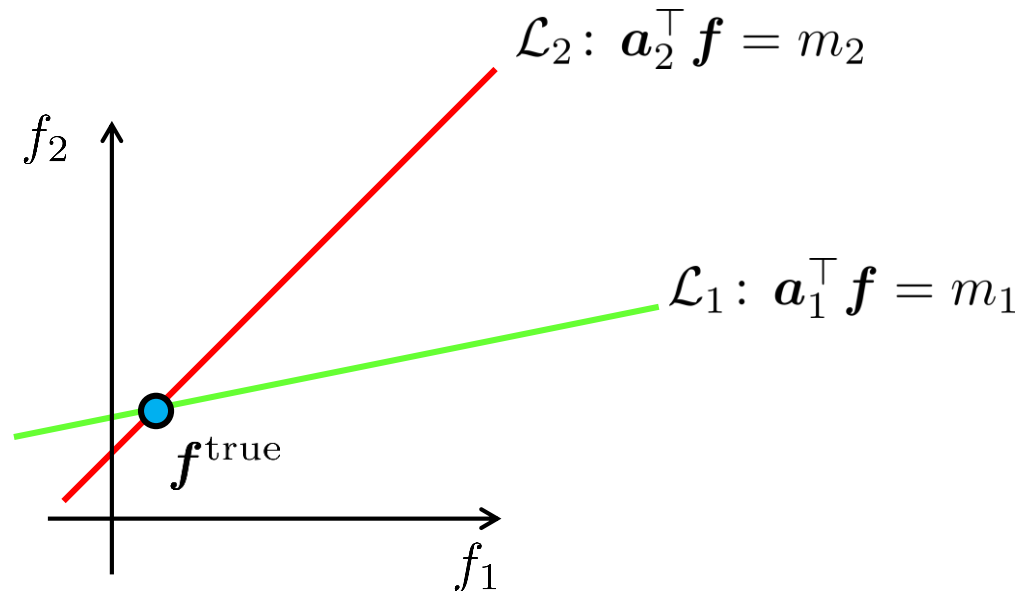
Algebraic reconstruction technique (ART) [Gordon R., 1970]



- Look for an image with small residuals

$$r = m - Af \approx 0$$

- Influence of noise

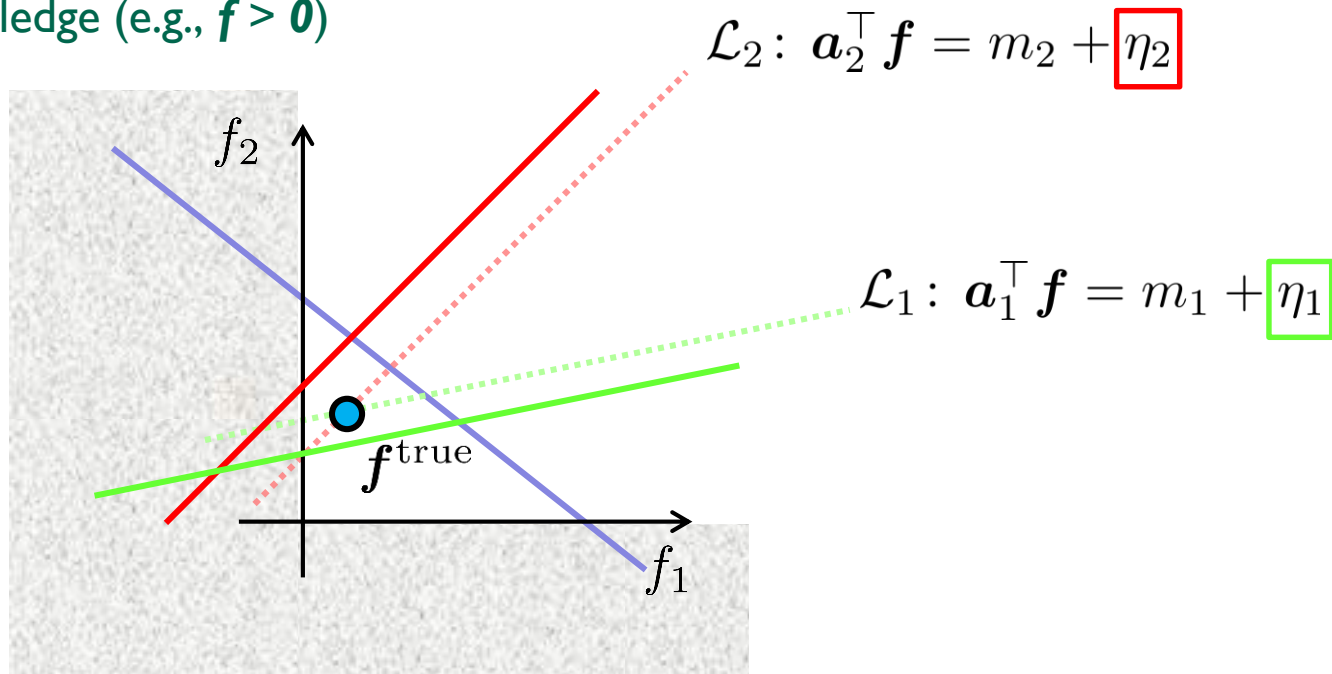


- Look for an image with small residuals

$$r = m - Af \approx 0$$

- Influence of noise

- ❖ More measurements (i.e., $M > N$)
- ❖ Prior knowledge (e.g., $f > 0$)



➤ Typical cost functions

$$\min_f \mathcal{D}(\mathbf{f}, \mathbf{m}) + \lambda \mathcal{R}(\mathbf{f})$$

Data fidelity

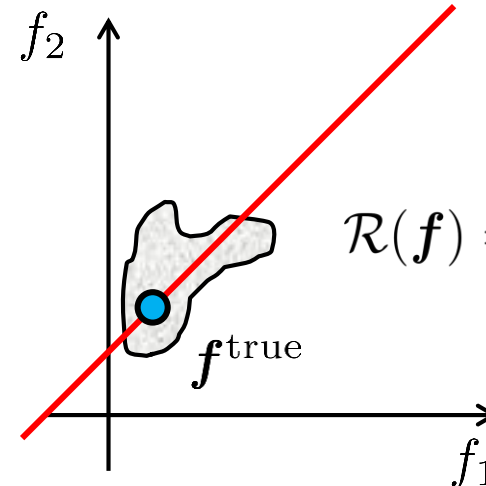
Regularization (prior)

- ❖ Data fidelity is related the noise model/measurements confidence.
E.g.

$$\mathcal{D}(\mathbf{f}; \mathbf{m}) = \|\mathbf{m} - \mathbf{A}\mathbf{f}\|_W^2$$

$$\mathcal{D}(\mathbf{f}; \mathbf{m}) = \text{KL}(\mathbf{m}, \mathbf{A}\mathbf{f})$$

- ❖ Regularization convey prior knowledge about the solution.



$$M \ll N$$

$$\mathcal{R}(\mathbf{f}) = \begin{cases} 0 & \text{if } \mathbf{f} \in \mathcal{X} \\ \infty & \text{otherwise} \end{cases}$$

➤ Typical regularizers

❖ Quadratic / Tikhonov regularization

$$\mathcal{R}(\mathbf{f}) = \|\mathbf{f}\|_2^2$$

... leads to

$$\mathbf{f}^* = \mathbf{A}^\top (\mathbf{A}\mathbf{A}^\top + \lambda \mathbf{I}_M)^{-1} \mathbf{m}$$

❖ Parsimony-promoting

$$\mathcal{R}(\mathbf{f}) = \|\Psi \mathbf{f}\|_1$$

... requires iterative algorithms

$$\mathbf{z}^{(k)} = \mathbf{f}^{(k-1)} - \eta \mathbf{A}^\top (\mathbf{A} \mathbf{f}^{(k-1)} - \mathbf{m})$$

$$\mathbf{f}^{(k)} = \text{prox}_{\lambda \mathcal{R}}(\mathbf{z}^{(k)})$$

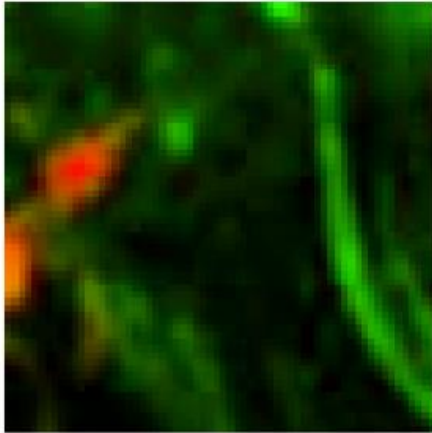
gradient of
data fidelity

proximal
operator of
regularizer

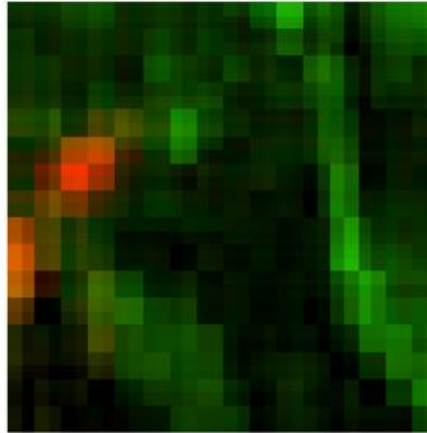
➤ Illustrative results

$N = 64 \times 64$ image
 $M = 333$ measurements
 $N / M \approx 8\%$

Ground-Truth



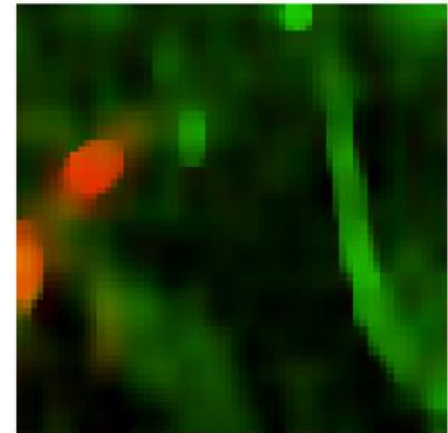
$$\mathcal{R}(f) = \|f\|_2^2$$



++ Analytical solution
(fast computation)

-- Image quality

$$\mathcal{R}(f) = \|\nabla f\|_1$$



-- Iterative algorithms
(time consuming)

++ Image quality

➤ **Our dream is to find**

$$\mathcal{H}^* : \mathbb{R}^M \mapsto \mathbb{R}^N \text{ such that } \mathcal{H}^*(\mathbf{m}) = \mathbf{f}^{\text{true}}$$

... able to reconstruct well any image, i.e., something like

$$\mathcal{H}^* \in \arg \min_{\mathcal{H}} \frac{1}{L} \sum_{\ell} \|\mathcal{H}(\mathbf{m}^{\ell}) - \mathbf{f}^{\ell}\|_2^2$$

Minimum mean square error (MMSE) estimator

... A scary problem

➤ **We have to reduce the dimension of the solution space**

❖ E.g.,

$$\mathcal{H}(\mathbf{m}) = \mathbf{W}\mathbf{m} + \mathbf{b},$$

Linear MMSE estimator

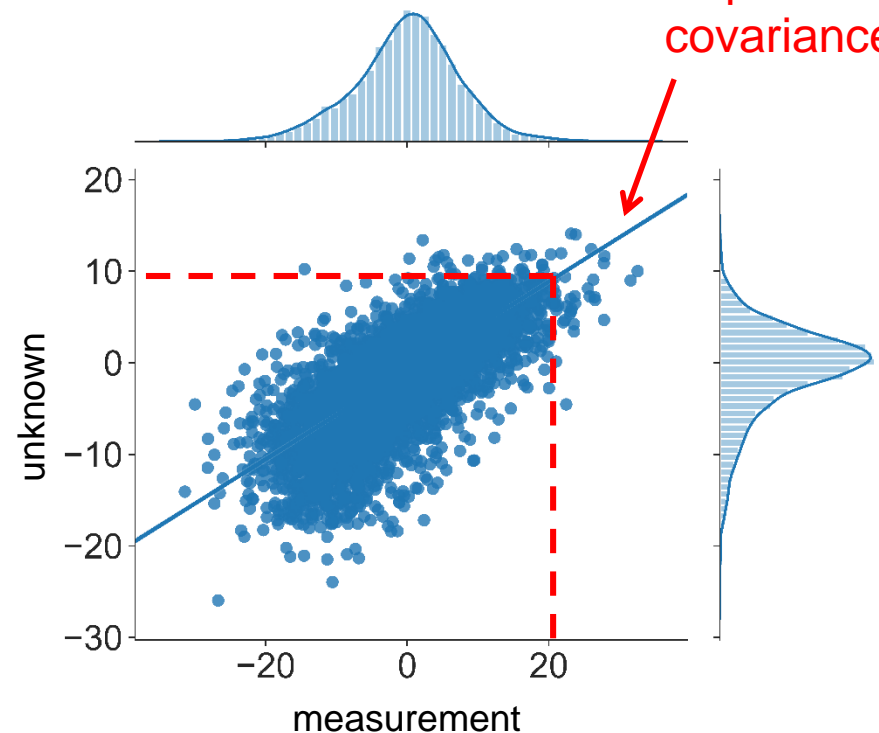
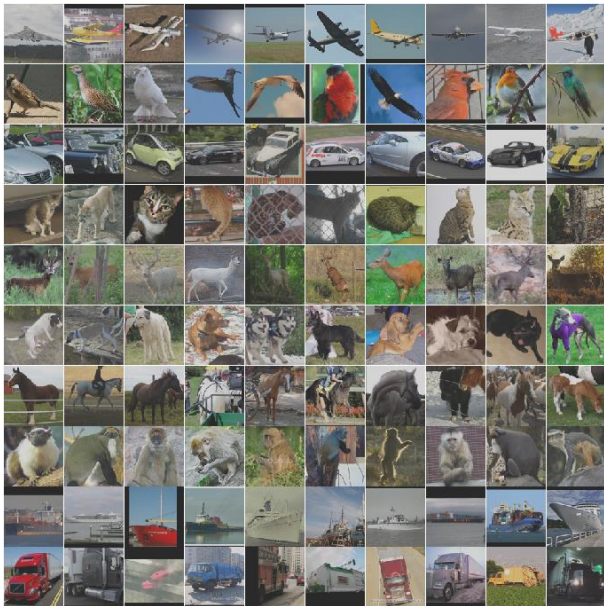
➤ Linear MMSE

$$f^* = \bar{f} + \Sigma_{f,m} \Sigma_m^{-1} (m - \bar{m})$$

Covariance between
measurements and
unknowns

Covariance of
measurements

slope →
covariance



- Learning approaches only reduce the dimension of the solution space to a family of non linear mappings

$$\theta^* \in \arg \min_{\theta} \frac{1}{L} \sum_{\ell} \|\mathcal{H}(\theta; m^{\ell}) - f^{\ell}\|_2^2$$

❖ Training phase

- Image-measurement pairs $\{f^{(\ell)}; m^{(\ell)}\}_{1 \leq \ell \leq L}$
- Loss (e.g., mse)
- Optimization machinery (i.e., through PyTorch/TensorFlow)

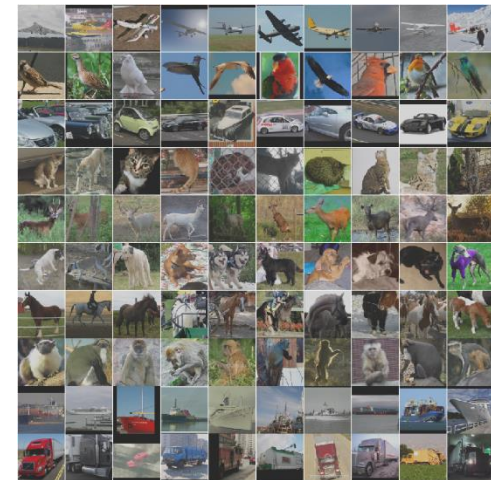
D.P. Kingma and J.L Ba,
ICRL, 2015 (> 215k citations)

A. Paszke *et al.*, NEURIPS,
2019 (> 22k citations)

❖ Reconstruction phase

$$f^* = \mathcal{H}_{\theta^*}(m)$$

STL-10 dataset



➤ Pros

❖ Reconstruction performance

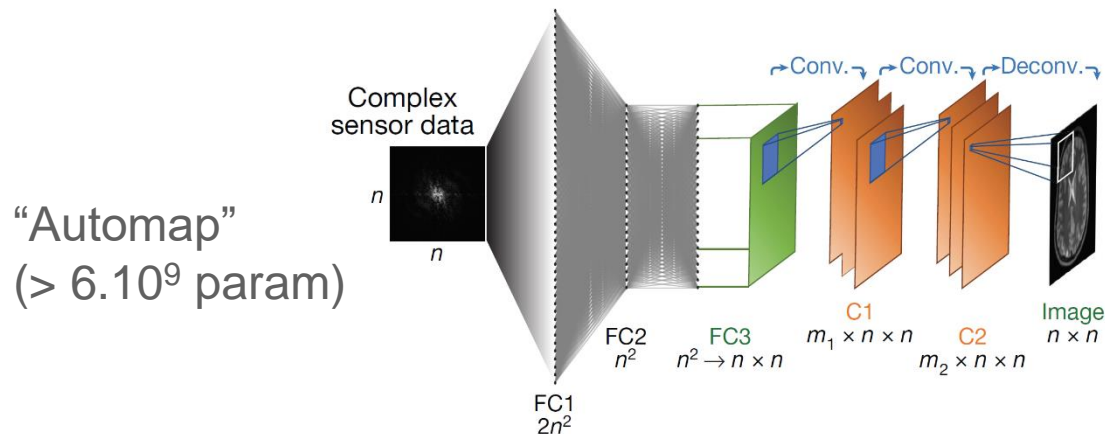
- Empirically excellent (i.e., almost always outperform optimization-based approaches)

❖ Computation times

- Training phase is slow, i.e., several hours or days
- Inference is fast, i.e., tens or hundreds of milliseconds

➤ Cons

- ❖ No reconstruction guarantees (*mathematicians don't like it*)
- ❖ Black box (*radiologists don't like it*)
- ❖ Practical issues
 - How to choose the model?

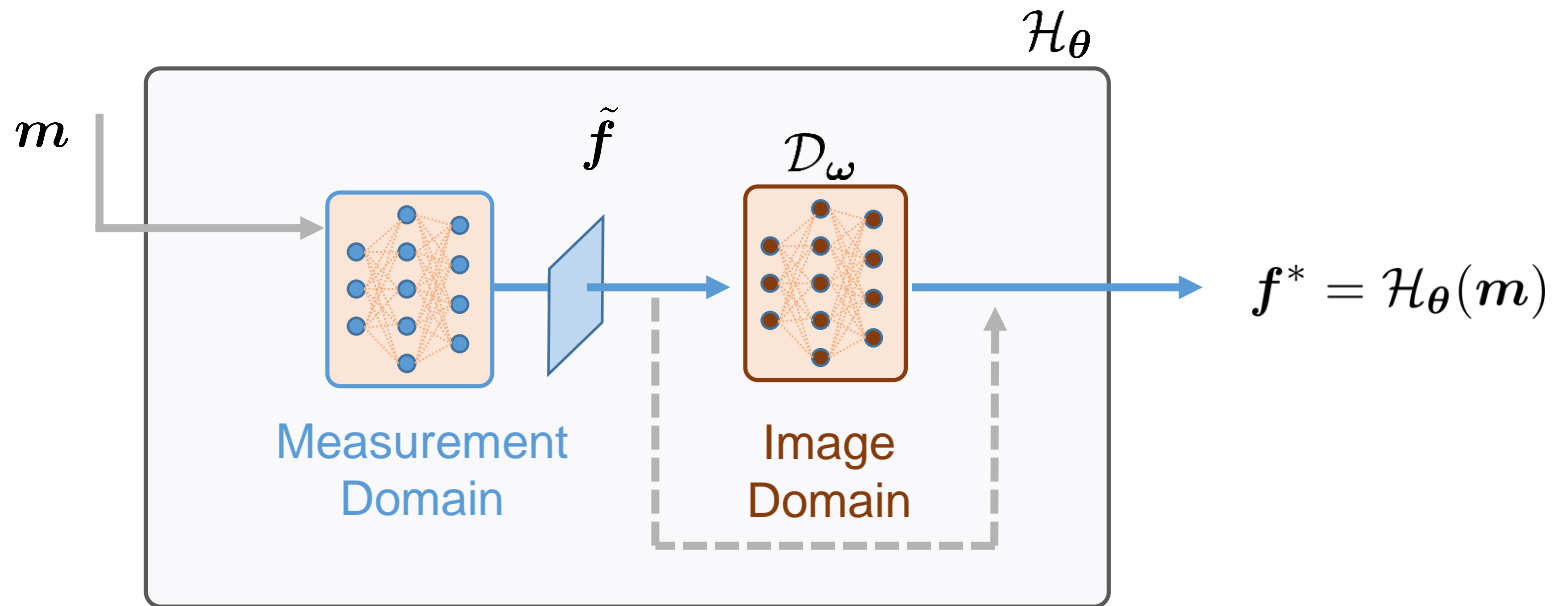


[B. Zhu et al., Nature Letters, 2018] ($> 1.5k$ citations)

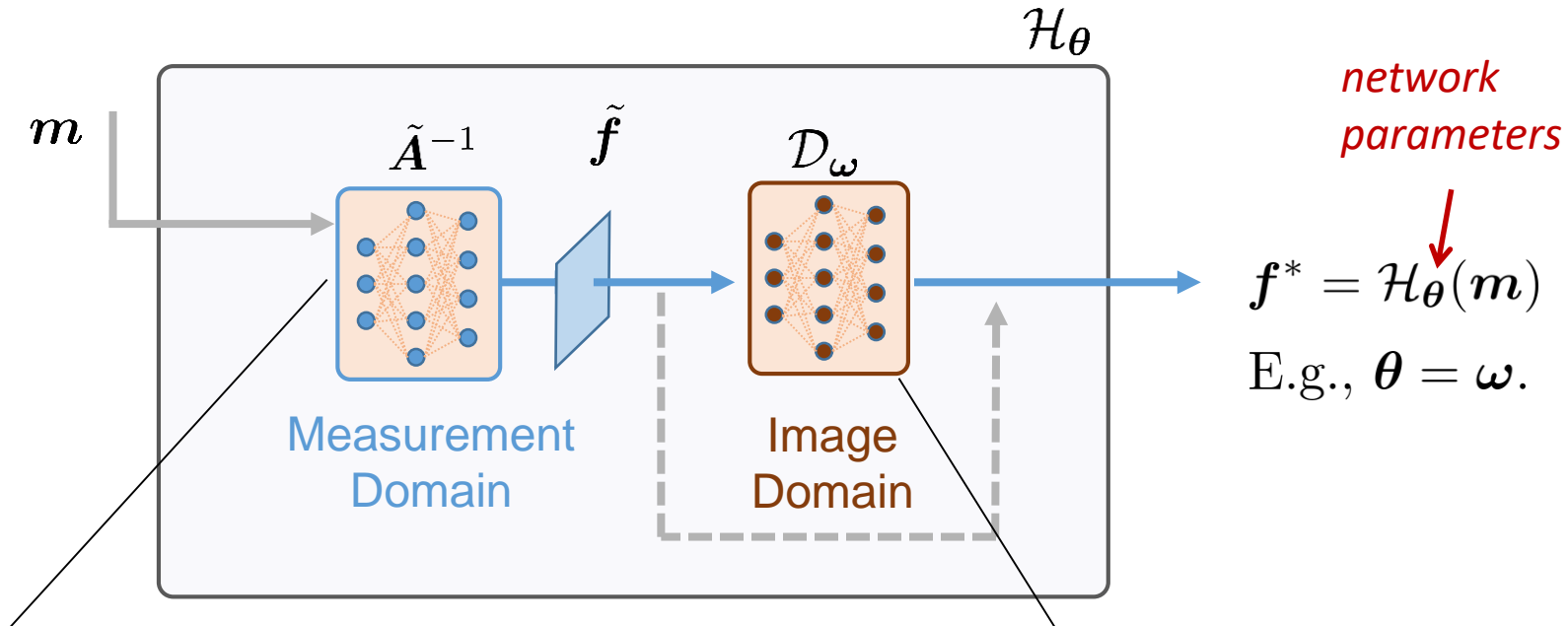
➤ Direct methods

$$\tilde{f} = \tilde{A}^{-1}m$$
$$f^* = \mathcal{D}_\omega(\tilde{f}) + \tilde{f}$$

where \tilde{A}^{-1} is an approximate inverse of the forward, i.e., $\tilde{A}^{-1}A f \approx f$



➤ **Direct methods with frozen layers**



```
Atilde = nn.Linear(..., bias=False, ...)
Atilde.weight.requires_grad = False
```

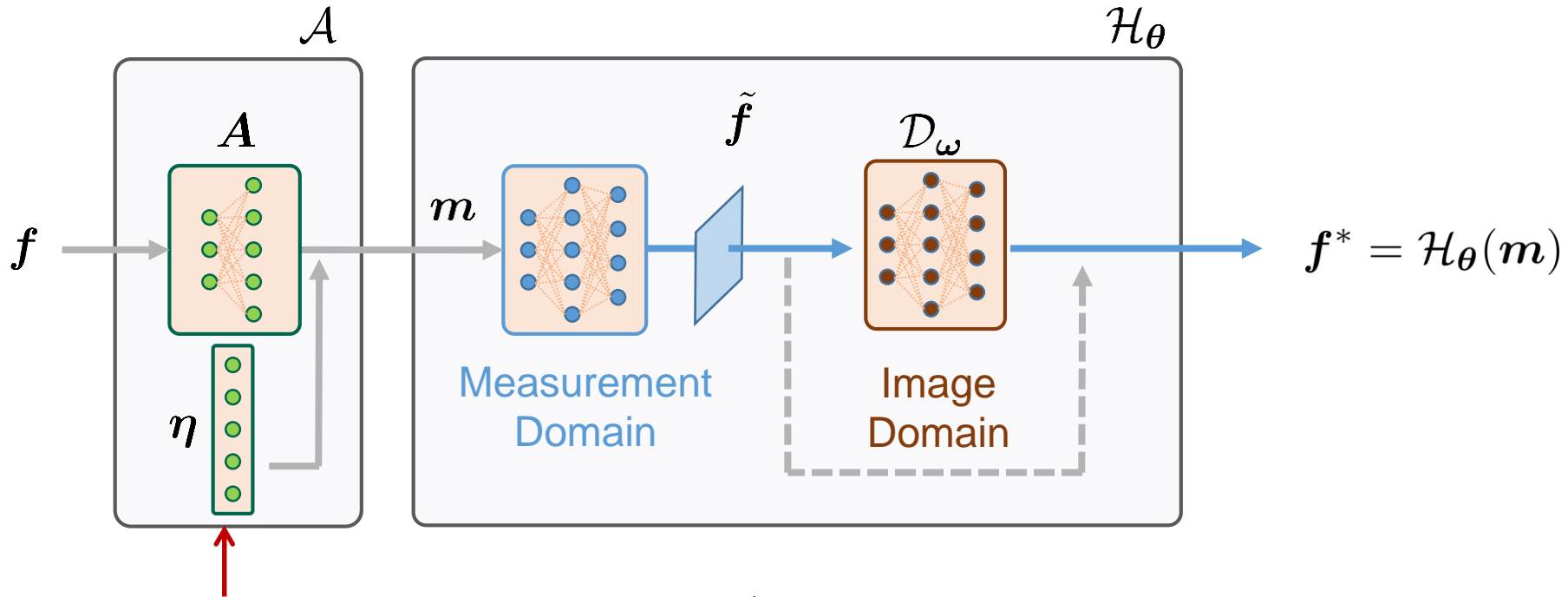
$$\tilde{A}^{-1} = A^\top$$

$$\tilde{A}^{-1} = A^\dagger = A^\top (AA^\top)^{-1}$$

$$\tilde{A}^{-1} = A^\top (AA^\top + I)^{-1}$$

```
D = nn.Module(...)
requires_grad = True
```

- **Direct methods with a physical module (no need for meas/image pairs)**



physical module

$$\theta^* \in \arg \min_{\theta} \frac{1}{L} \sum_{\ell} \|\mathcal{H}_{\theta}(m^{\ell}) - f^{\ell}\|_2^2$$

$$\mathcal{A}(f) = Af + \eta$$

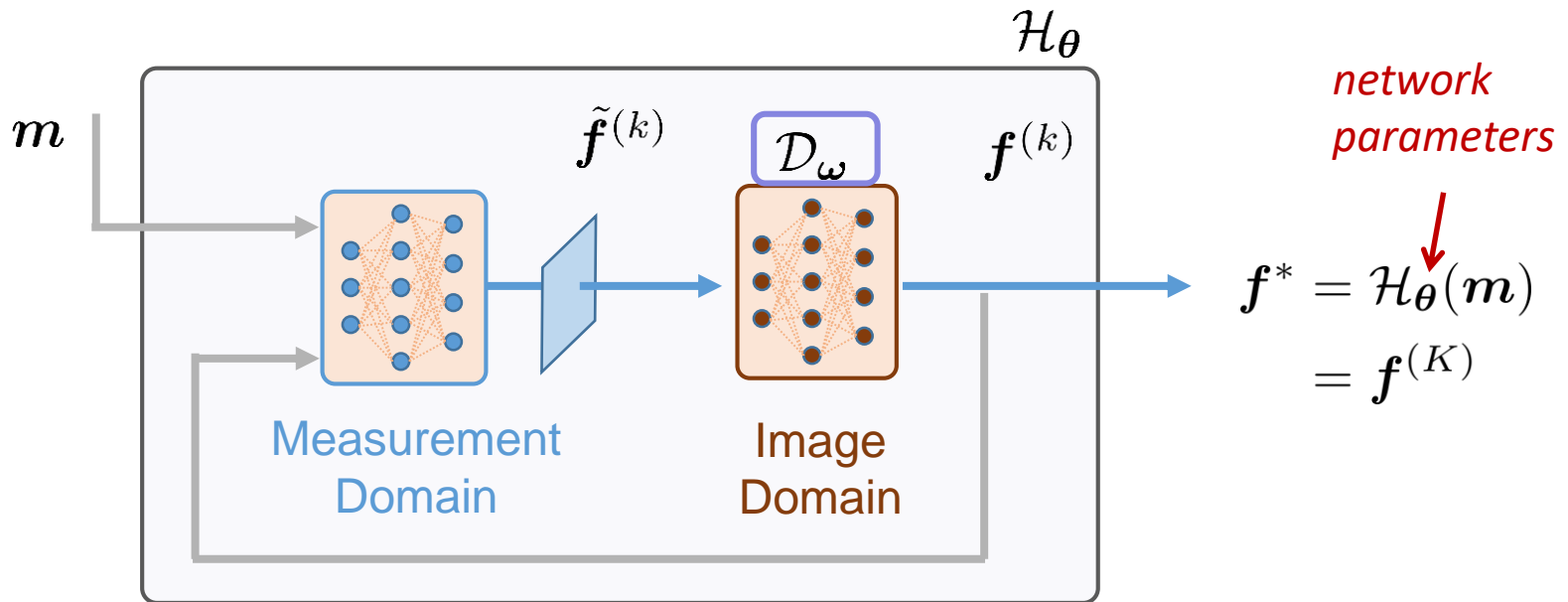
$$\theta^* \in \arg \min_{\theta} \frac{1}{L} \sum_{\ell} \|(\mathcal{H}_{\theta} \circ \mathcal{A})(f^{\ell}) - f^{\ell}\|_2^2$$

➤ **Unrolled / Plug&Play methods**

$$z^{(k)} = f^{(k-1)} - \eta \mathbf{A}^\top (\mathbf{A} f^{(k-1)} - m)$$

$$f^{(k)} = \text{prox}_{\lambda \mathcal{R}}(z^{(k)}) \quad \text{data fidelity}$$

proximal operator



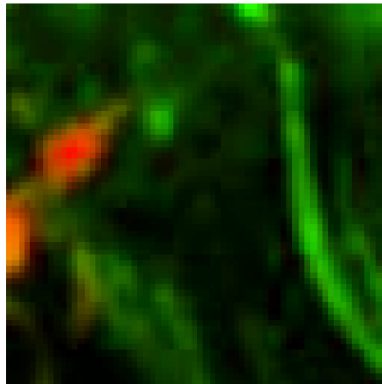
Parameters can be shared across iterations or not

E.g., $\theta = \omega$,
or $\theta = [\omega^{(1)}, \dots, \omega^{(K)}]$.

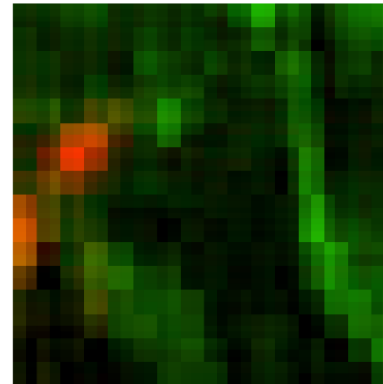
➤ **Illustrative results (option #2 vs option #3)**

$N = 64 \times 64$ image
 $M = 333$ measurements
 $N / M \approx 8\%$

(a) Ground-Truth

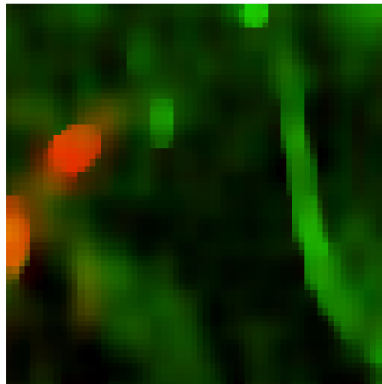


(b) Pseudo Inverse



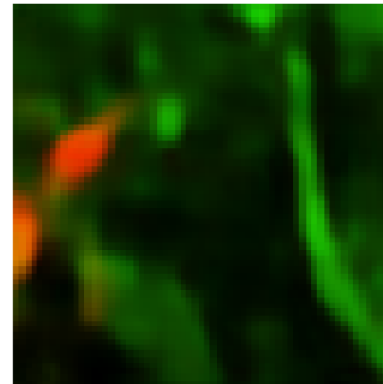
$$\mathcal{R}(f) = \|f\|_2^2$$

(c) Total Variation



$$\mathcal{R}(f) = \|\nabla f\|_1$$

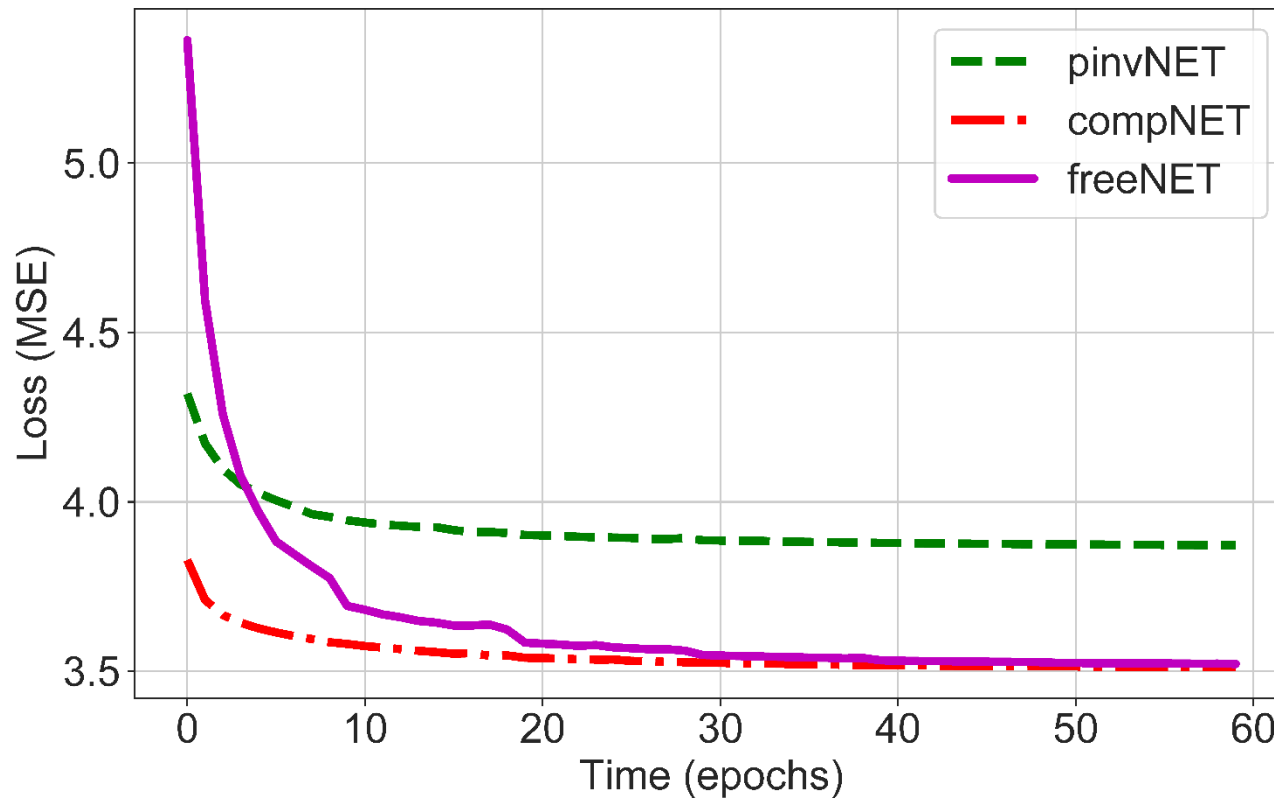
(d) compNET



$$f^* = \text{CNN}(\mathbf{A}_{\text{mmse}} m)$$

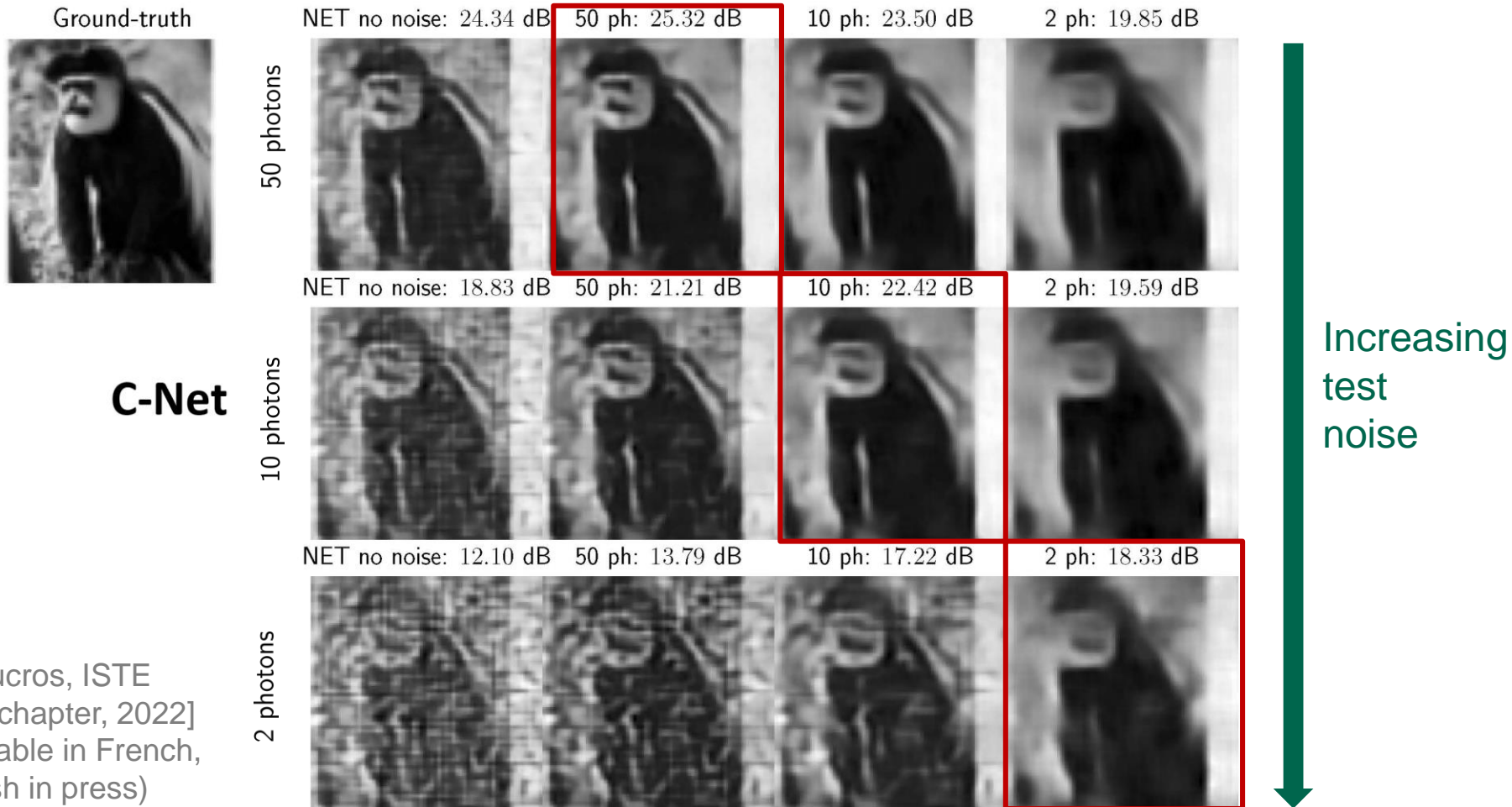
- **STL-10 (training: ~100k images; test: 8k images)**

$$\sum_{\ell \in \mathcal{I}_{\text{test}}} \|f^{(\ell)} - \mathcal{H}_{\theta}(m^{(\ell)})\|^2$$



➤ Noise robustness

Increasing training noise



[N. Ducros, ISTE Book chapter, 2022] (Available in French, English in press)

- **Data driven approaches for image reconstruction based on DL are**
 - ❖ Powerful!
 - ❖ No longer black boxes
- **Unrolled algorithms**
 - ❖ Usually require fewer parameters than their direct counterparts
 - ❖ More interpretable
- **Warning**
 - ❖ Noise is still an issue.
 - Train with noise
 - Evaluate the robustness to noise level deviations

Hands-on session at 2 pm!